In cervical spondylotic myelopathy (CSM) there is dysfunction of the spinal cord because of degenerative changes in the spine. The pathophysiology of neural loss is still a subject of some debate. Essentially there are two major mechanisms which cause myelopathy: direct compression of the cord and ischemic changes because of alterations in the local blood flow [10, 14, 41, 42, 55]. Since studies have demonstrated that the pathology of CSM is located predominantly anteriorly [47], it seems logical to approach the spine where the lesion is and choose an anterior approach. Removal of extruding intervertebral disc, spurs, osteophytes and calcified posterior longitudinal ligament relieves the compression of the anterior cord and improves to some extent the blood supply to the cord. The surgical approach as described by Smith and Robinson [86] covers the area between the vertebral bodies of C2 and T1. In patients with long slender necks the vertebral body of T3 may be within reach by this approach. The Smith and Robinson approach allows atraumatic dissection of the anterior aspect of the cervical spine. There is a low potential risk for injuries of the esophagus, trachea, the recurrent laryngeal nerve, and the carotid artery. The direct visualization of the offending pathology allows atraumatic and extensive decompression.

Abstract Cervical spondylotic myelopathy is a clinical entity that manifests itself due to compression and ischemia of the spinal cord. The goal of treatment is to decompress the spinal cord and stabilize the spine in neutral, anatomical position. Since the obstruction and compression of the cord are localized in front of the cord, it is obvious that an anterior surgical approach is the preferred one. The different surgical procedures, complications, and outcome are discussed here.

Keywords Cervical spondylotic myelopathy · Anterior surgery · Fusion · Decompression
ment of degenerative conditions of the cervical spine. This procedure is predictable with respect to decompression and symptom relief. It is suitable for addressing stenotic changes at single or multiple levels. Restoration of the intervertebral height and the lordotic curvature is possible when approaching each level separately (Fig. 1). On the other hand, this may result in increased risk for symptomatic pseudarthrosis because of the large number areas to fuse [39, 54, 83]. Since the degenerative changes in CSM cover a large area of the subaxial spine, corpectomy and grafting may be advocated [9, 10, 58]. Various terms have been adopted to describe the partial vertebral body resection, including complete or partial vertebrectomy, anterior corpectomy, and partial corpectomy. Basically all the terms refer to a partial resection of the vertebral body without removal of the transverse processes, pedicles, lateral masses, or other posterior elements. Resection of the lateral part of the uncovertebral joints must also be avoided to prevent injury of the vertebral artery. After decompression the spine must be reconstructed using strut grafts or artificial devices with or without internal fixation [21, 31, 36, 38, 44, 51, 63, 66, 94, 95].

**Surgical technique**

In monosegmental decompression and stabilization it is essential to have sufficient view of the posterior part of the intervertebral space. After excision of the intervertebral disc and resection of the posterior longitudinal ligament the osteophytes must be recognized and entirely removed. Use of the diamond bur is recommended, together with Kerrison rongeurs and curettes. To ensure sufficient distraction of the intervertebral space a strong interlaminar spreader may be used. Use of the Caspar distractor is also recommended. It must be recognized that this distractor has limited ability to mobilize collapsed segments. When performing partial vertebrectomy it is essential to have a wide trough, positioned symmetrically in the mid-

line. The width of the trough is up to 18 mm and may include the medial part of the uncovertebral joints [65]. Some authors do not advocate entire removal of the mid-section of the posterior wall of the vertebral body [33].

### Grafts, bone substitutes, devices, internal fixation

Structural autografts harvested from the anterior iliac crest or from the fibula are used in anterior fusion of the cervical spine. The grafts must enhance stability and substitute for the regenerative capacity of bone. Fresh autologous grafts possess some osteogenic potential and have osteoinductive and osteoconductive properties [62]. Structural corticocancellous grafts from the anterior iliac crest are commonly used, and their mechanical strength is greater than that of the posterior crest [89]. Iliac crest grafts are used in mono- and bisegmental interbody fusion and also after corpectomy involving no more then two levels. They are considered the biological and biomechanical standard for mono- and bisegmental reconstruction of the anterior cervical spine [3, 11, 17, 73, 75, 86, 98, 102, 103, 107]. In longer fusions after corpectomies a structural fibula graft is appropriate. There are different techniques for stabilizing the strut graft within the decompressed site [7, 47, 78, 105, 106]. Vascularized fibula grafts may accelerate the process of fusion in the case of multiple vertebrectomies [80, 100]. Additional internal fixation may provide immediate intrinsic stability in long strut graft constructs [15, 16, 46, 67, 92]. There are disadvantages when using autologous grafts such as potential donor site morbidity, increased operative time, and hospital stay.

To avoid these disadvantages allografts may be considered. There are also disadvantages concerning the use of allografts, such as risk of transmitting infections from the donor, prolonged healing, and compatibility problems [26, 30, 34, 49, 74, 82, 88, 99, 107]. The use of allografts in multilevel reconstructions is associated with a nonunion rate up to 41%. This nonunion rate is significantly higher than that with autologous grafts, which is estimated at 27% [24]. Allografts may be preserved as fresh-frozen or freeze-dried [27, 52, 87]. Both processes are effective in suppressing antigenicity and retain some osteoinductive ability and osteoconductive properties [62]. Other methods, including sterilization with ethylene oxide gas and high-dose γ-irradiation are effective but decrease significantly the osteoinductive properties and mechanical integrity of the graft [69, 81].

 Demineralized bone matrix is composed material, consisting from some collagen proteins and bone growth factors [45]. There are some osteoinductive and osteoconductive properties established [81]. Since demineralized bone matrix lacks mechanical properties that resist forces, it is not suitable for reconstruction of large defects in the cervical spine.
Bioceramics are calcium phosphate materials processed by sintering. Hydroxyapatite and β-tricalcium phosphate are examples of the ceramics which may be used in reconstructive surgery. Hydroxyapatite is almost unresorbable while β-tricalcium phosphate degrades and resorbs 6–12 weeks after surgery [40, 70]. The bioceramics are mechanically stable, but the material is brittle and not suitable for use as a stand-alone device. Combined with a rigid anterior fixation bioceramics may be very successful in anterior interbody fusion [91].

**Interposition devices (cages)**

The introduction of interbody spacers, so-called cages, is the answer to donor site morbidity and optimization of the fusion construct. There are two major types of cages: threaded hollow cylinders and rectangular cages. There is a fundamental difference in mode of action. The threaded cages are introduced and screwed through the endplates of the vertebral bodies, whereas the rectangular cages mimic the intervertebral space dimensions and are in accordance with the anatomy of the endplates. In long fusions cylindrical mesh cages are employed, filled with autologous bone. Most cages are made of titanium, carbon fiber of poly-ether-ether-keton. The cages may be used empty or filled with autologous bone or bone substitutes. Good results have been reported by different authors [35, 50]. Our experience with rectangular cages made of poly-ether-ether-keton and filled with β-tricalcium phosphate (Cervios and Chronos, Mathys Medical, Bettlach, Switzerland) is extremely good. In a study to be published, we report that the TCP inserts are resorbed and restored by trabecular bone within 9 months after surgery (Fig. 2).

**Internal fixation**

Internal fixation after decompression and fusion of the cervical spine provides high intrinsic stability of the construct, maintains alignment, and allows early functional recovery [2]. However, there is no substantial evidence to demonstrate higher fusion rates in plated fusion [1, 18, 96, 109, 110]. On the other hand, there are reports of improved maintenance of the sagittal profile of the spine after instrumented fusion [48, 93, 97]. Internal fixation is used by many surgeons today for mono- and bisegmental anterior interbody fusion [29, 76, 85]. In multilevel fusion after corpectomy (three or more levels), however, high rates of complications and pseudarthrosis have been reported [12, 20]. Di Angelo et al. [19] described the adverse effect of rigid anterior fixation on the stability of the construct. They concluded that the anterior plating reverses strut graft loading mechanics and excessively loads the graft in retroflexion. The stress shielding phenomenon has been observed by using rigid plates and screws with fixed angular orientation [108]. To improve some shortcomings of rigid fixation systems the concept of dynamic fixation has been introduced [1]. The “old” Caspar plates (Aesculaap, Braun, Tuttlingen, Germany) and Orozco (Synthes, Switzerland) are the first examples of noncontrolled dynamic fixation on the cervical spine. Numerous different systems have been introduced to permit controlled dynamization of anterior fixation. Early reports are promising but not sufficiently convincing.

**Complications**

Mono- or bisegmental interbody fusion is usually not complication prone. The major complaints with autologous iliac crest grafts are from the donor site. Morbidity of up to 25% has been reported [79], and residual pain may persist for as long as 24 months after surgery [6]. The major advantage with cages filled with bone substitutes is the avoidance of any donor site morbidity. Multisegmental corpectomy and strut graft reconstructions contribute to the majority of complications regarding anterior surgery of the cervical spine. Some authors have reported perioperative complication rates up to 60% [8, 15, 53, 58, 68, 71, 78, 94, 106]. Most of these are due to inadequate soft tissue exposure and careless handling of vessels, nerves, and esophagus. Neural injuries are usually transient and involve the relatively short C5 nerve roots [77]. Complica-
tions related to bone grafting after multiple corpectomies are very common [7, 13, 24, 39]. Graft extrusion has been reported in 5–20%, even when internal fixation is used [25]. There are even reports of increased complication rate when using internal fixation [58, 68]. In instrumented multilevel corpectomies the construct failure that is observed is due to pistoning of the graft. This occurs because rigid anterior plating reverses graft-loading mechanics and excessively loads the graft in retroflexion. This load is higher then the resistive strength of the endplates, and therefore the strut graft subsides [4, 5, 28, 61, 101]. Using titanium mesh cage, Hee et al. [38] reported a high fusion rate of 95% for multilevel corpectomies but still an overall complication rate of 33%.

**Outcome**

Since there are no reliable data on the natural history of CSM, its treatment remains controversial. However, the anterior decompression and stabilization of the stenotic cervical spine reliably arrests myelopathy progression, and there is measurable objective improvement [7, 13, 15, 23, 25, 37, 57, 59]. Other authors report even a cure rate of excess of 50% and a regression rate of 5% [77]. A mean morbidity rate of 31% has been reported, which emphasizes the challenging nature of this kind of surgery [64, 84, 92, 106]. In an independent matched-cohort analysis comparing corpectomy vs. laminoplasty for multiple cervical myelopathy Edwards et al. [22] reported similar clinical outcome in the two cohorts, with fewer complications in the laminoplasty group. In the long term surgical benefits are maintained but functional capacity deteriorates. This is age related and may be an expression of a slow progression of cord dysfunction [104]. The surgical outcome from anterior decompression of the myelopathic spine is predictable. In monosegmental procedures the fusion rate is high, and the pseudarthrosis rate ranges from 4 to 6%. In the multilevel segmental fusion the pseudarthrosis rate increases due to the increased number of surfaces to fuse [39, 55, 83]. Preliminary experience in our clinic with anatomically shaped cages suggests a significant decrease in pseudarthrosis rate in multisegmental decompression and fusion. After solving the early complications with strut grafts in multilevel corpectomies the surgical outcome seems to be successful. In different series fusion rates above 90% have been reported without respect to plating as well [25, 23, 43, 72, 106].

In conclusion, the anterior approach to the myelopathic cervical spine is a logical answer to a specific pathological substrate. It is a challenging and rewarding surgery, which must be tailored to the individual patient.

**References**


